

How to verify DIR? Can we use DIR in the clinic and for which purpose?

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Validation of method

- Physical phantoms
- **Digital phantoms**
- **Exogenous fiducials** ullet
- Internal anatomical landmarks
 - Pooling of ground truth data
 - Grand challenges
- Visual Inspection

Verification during intervention/therapy etc

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5 naining:

- Exogenous fiducials
- Internal anatomical landmarks
- understanding limitations Visual Inspection

Experimental validation and clinical evaluation

3



Anthropomorphic phantom: <u>http://medicalphysicsweb.org/cws/article/research/53748</u>

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Alignment of temporal sequences of DCE-MRI



Difference of original images

Free form deformations using B-splines with normalised mutual information as a similarity measure



Difference of aligned images

Rueckert et al IEEE-Trans Med Imag, 1999



From Free-Form Deformation (FFD) to Fast Free-Form Deformation (F³D)

- Update all control points for each resampling
- Parzen Window estimation of Joint Histogram
- Convolution of gradient field of the cost function (NMI)
- Conjugate Gradient
 Optimisation
- 10 fold speed up from CPU to GPU implementation

Open source code available at: http://www.niftk.org



Modat et al, Computer Methods and Programs in Biomedicine, 2010



Whole breast

Schnabel et al IEEE-TMI 2003, Tanner et al Med Phys 2006



TLED-Reg Motivation

• As many atrophy rates as algorithms:







CMIC seminar, 29 october 2008, Marc Modat, m.modat@ucl.ac.uk

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iMRI facility at National Hospital, Queen Square, London



Planning and guiding avoidance of optic radiation Daga, Duncan, Ourselin et al IEEE TMI 2012



Pre-operative image and plan





Intra-operative image

Optic radiation



27% visual field loss



No visual field loss

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Breast Cancer & Clinical Needs



(FP7-ICT-2011-9)

- 78% Patients survive breast cancer for more than 10 years (Cancer Research UK)
- ~20% of patients undergoing lumpectomy have inadequate margins
- ~ 30% of patients suffer from suboptimal or poor aesthetic outcome

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Alignment of 3D prone and supine MR of breast via the unloaded configuration (simulated data)



Eiben et al Annals of Biomed Eng (2015)



Alignment of 3D prone MRI and supine CT of breast via synthetic MRI and the unloaded configuration (real data)



Eiben et al Annals of Biomed Eng (2015)



Surgical Simulator: Registration to 3D reconstructed visible surface



Magnetic Resonance Image (patient prone)

TRE 10.0mm (prone to supine) using user identified points from supine CT

Eiben PhD Thesis Nov 2015



CT SYNTHESIS IN THE HEAD & NECK REGION

- Challenges:
 - 1. Mixture of tissues
 - 2. Wide range of fields of view
 - 3. Large-scale postural changes











2. MULTI-ATLAS CT SYNTHESIS

Burgos et al., EJNMMI 2015





EXAMPLES OF CT SYNTHESIS IN THE HEAD & NECK

- Three pseudo CTs per subject
 - pCT_A, obtained using a single affine between the atlases and target
 - $-pCT_{R}$, obtained using the robust affine

1C





APPLICATION TO RADIOTHERAPY TREATMENT PLANNING

• Case study: dosimetry calculations

1C

- Dose volume histograms (DVH) in the planning target volume (PTV)
- Gamma analysis



DVH of PTV



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Image Directed Biopsy and Partial Prostate Ablation



- Multimodal MR to delineate focal cancer
- Biopsy
- Focal therapy (PDT or HIFU) delivered (via needle or transrectally) with transrectal ultrasound guidance





TRE 1.8mm (RMS) +/- 0.7mm



Clinical trial commenced, > 100 patients

EPSRC, NIHR i4i, Wellcome DoH HICF,

Hu Y, et al IEEE-tMI, 2011 + patent Hu y et al MedIA 2012

PRE-PROCEDURE



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Automatic generation of deformable organ models



Hu et al. Medical Image Analysis, 2012 and patent

Motion compensation in lung radiotherapy





Model error 1.7mm (RMS), slice thickness 1.5mm

McClelland et al Medical Physics 2006



Problem: Significant inter-fractional variation in breathing patterns

McClelland et al Phys Med Biol 2011





Lung registration using the NiftyReg package EMPIRE'10 (workshop at MICCAI 2010) http://empire10.isi.uu.nl



Marc Modat, Jamie McClelland and Sébastien Ourselin Centre for Medical Image Computing, University College London



Lung registration - Pipeline



• Preprocessing (Nifti format and masking)



- 1 global registration step (block-matching)
- 3 local registration step (F³D)



Lung registration - Local registration 3



TRE: landmarks 0.8mm and ranked 4th overall (slightly worse at lung boundaries and fissures)



Lung registration - Computation time

Computation time	CPU-based implementation	GPU-based implementation
Global registration	1.40(0.57)	NA
Local registration 1	1.28(0.47)	1.06(0.41)
Local registration 2	1.32(0.84)	$0.83 \ (0.36)$
Local registration 3	12.25(5.13)	1.56 (0.27)
Folding correction	1.16(0.57)	NA

Table 1: Mean computation time in minutes (and standard deviation) of the different registration stages.



What can still go wrong?

- Sliding of individual lobes
- Loss or gain of significant structure (tumour growth, reopening airways etc)
- Very large intensity changes can still throw the algorithm

In-room stereo video, KV and MV imaging with linac



Updated inter-fraction model from cone-beam CT



Simultaneous extraction of motion parameters and motion compensated cone-beam reconstruction



Original

Original + tumour outline

Synchronised in real-time with intra-fraction 4D skin surfaces (VisionRT)

Martin et al Phys Med Biol 2013



Combining Image Registration, Respiratory Motion Modelling, and Motion Compensated Image Reconstruction

Cine CT data – BH as static reference

McClelland et al WBIR 2014



Reconstruction of 4D MR images from volunteer with normal, irregular breathing

McClelland 2015

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Thank you

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