



# Modeling Breathing Motion

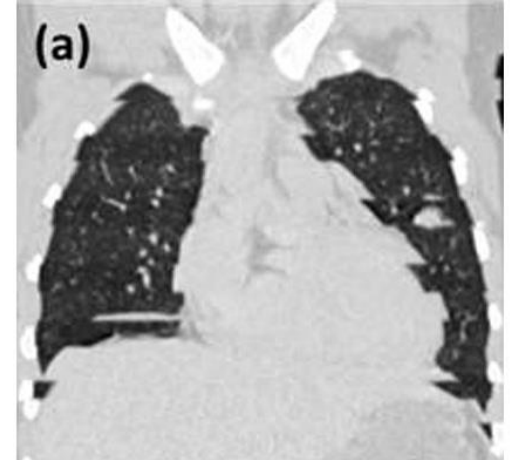
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# Analytical and Clinical Technique

- Change approach to “4D”
- Employ motion model
  - Mathematical description of motion
  - First iteration
    - Based on breathing amplitude and rate (originally volume and flow)
    - Linear in amplitude and rate
- Use images to measure motion
  - Simultaneous amplitude measurement
  - Motion information provides model parameters



# Motion Model

- Linear in amplitude ( $v$ ) and rate ( $f$ )
  - Rate models pressure disequilibria that are hypothesized to cause hysteresis

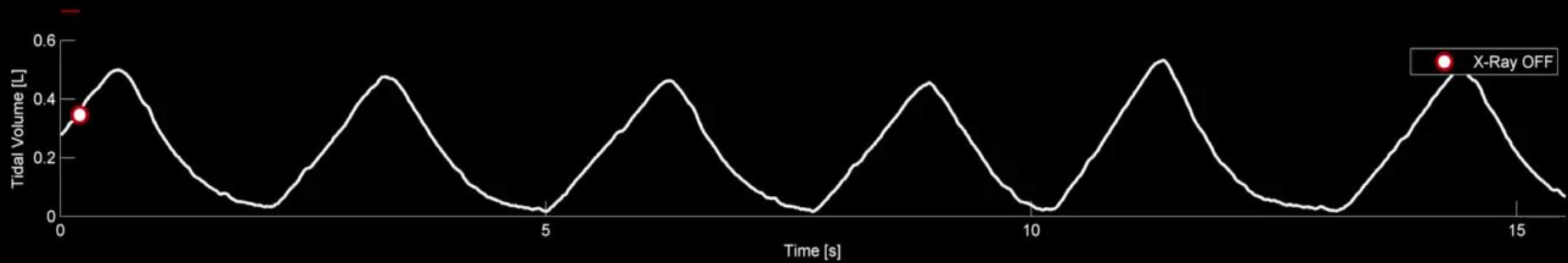
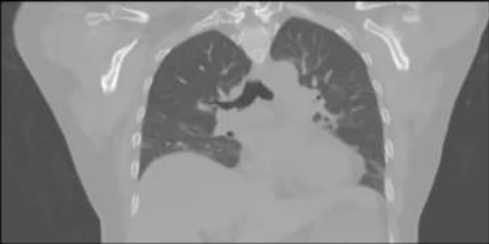
$$\vec{X}(v, f) = \vec{X}_0 + \vec{\alpha}(\vec{X}_0)v + \vec{\beta}(\vec{X}_0)f$$



# Imaging Requirements

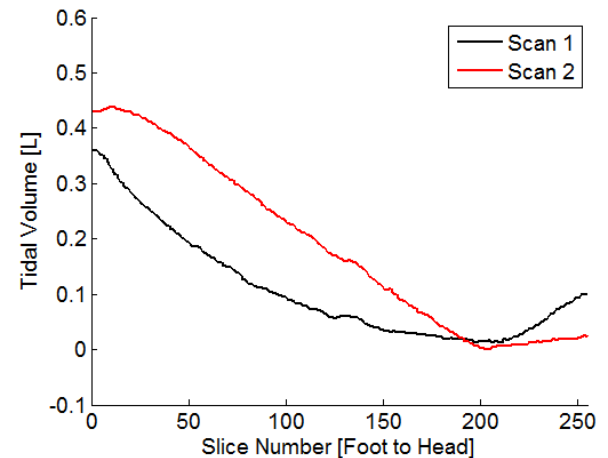
- $\alpha$  and  $\beta$  are voxel and patient-specific parameters
- The model needs data
- Data = where are the structures (voxels) as a function of amplitude and rate???
- Old technique: low-pitch helical or cine
- Insight: The images aren't for humans, they provide voxel attenuation and location

# 5DCT Imaging



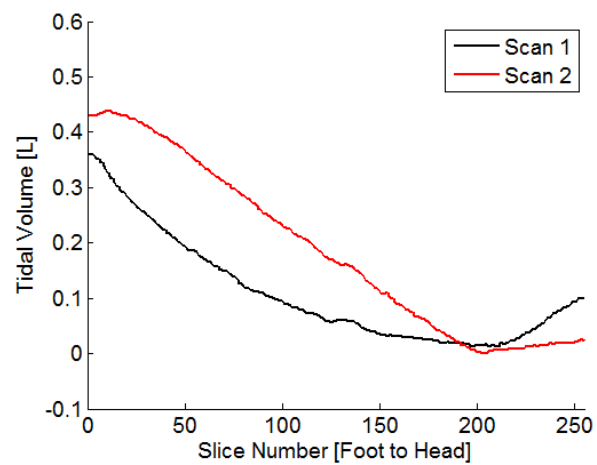
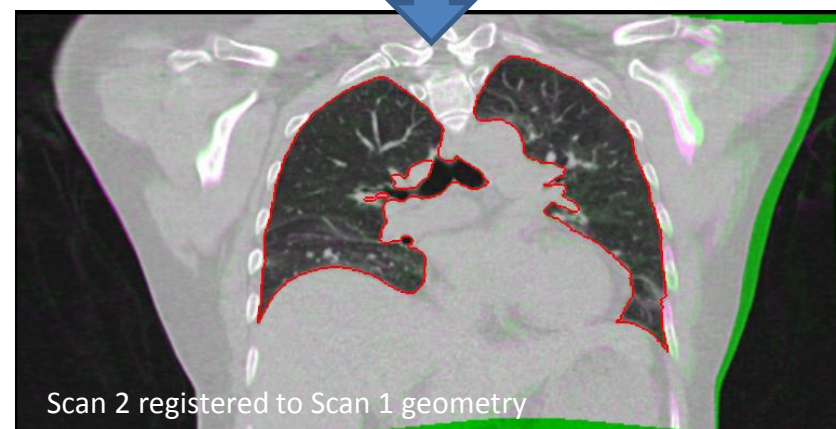
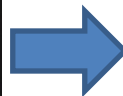
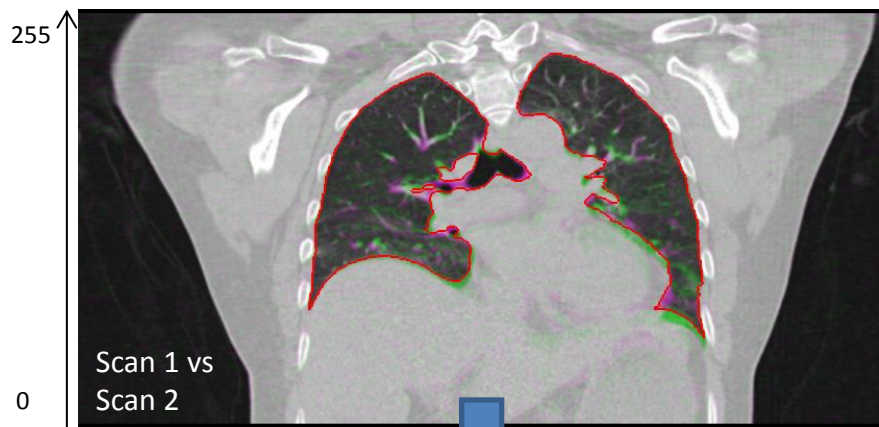
# Free Breathing Fast Helical

- Fast helical CT scan, 32 or 64-slice CT
  - Pitch 1.2, fastest rotation (approx 0.26s), 40 mAs, approx 1.5-2.5s per scan
- Scan both directions, minimum pause, whole lungs
- 25 times (research protocol)
- Measure breathing cycle during image acquisition
  - Bellows

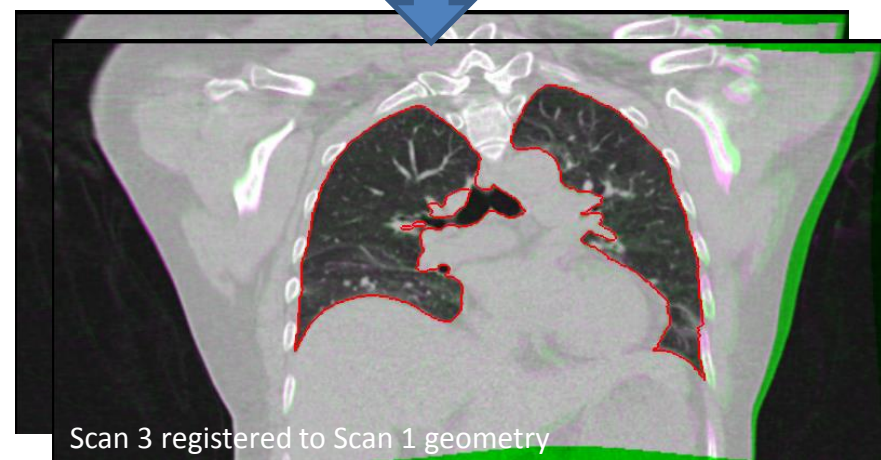
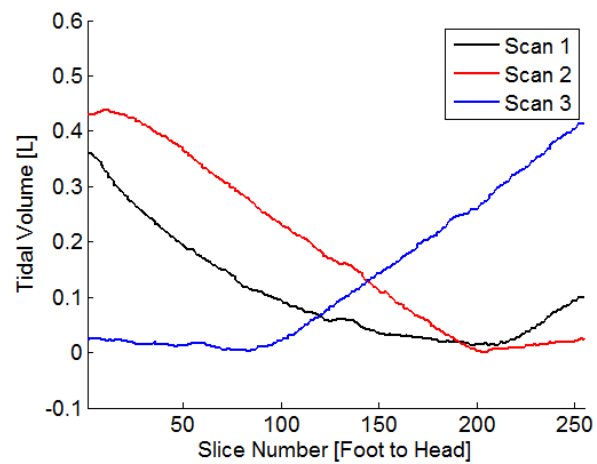
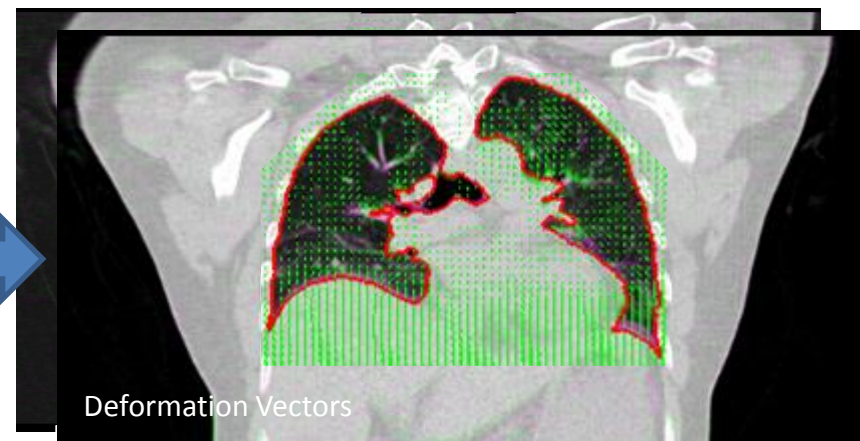
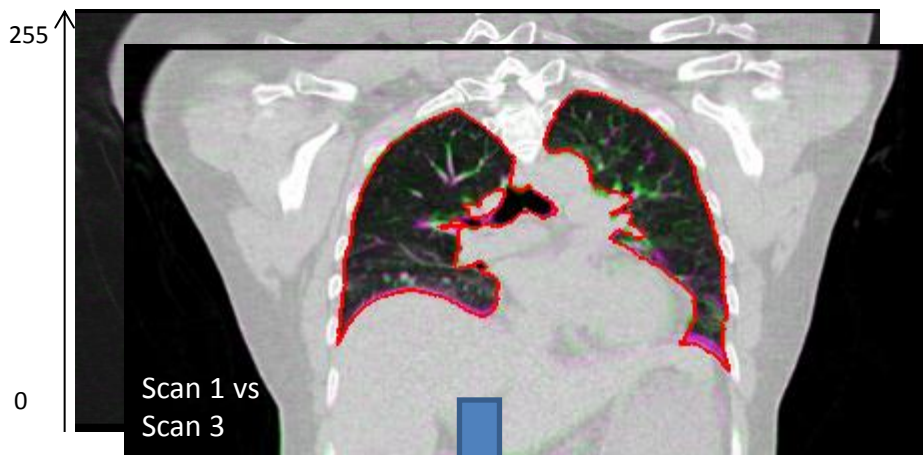


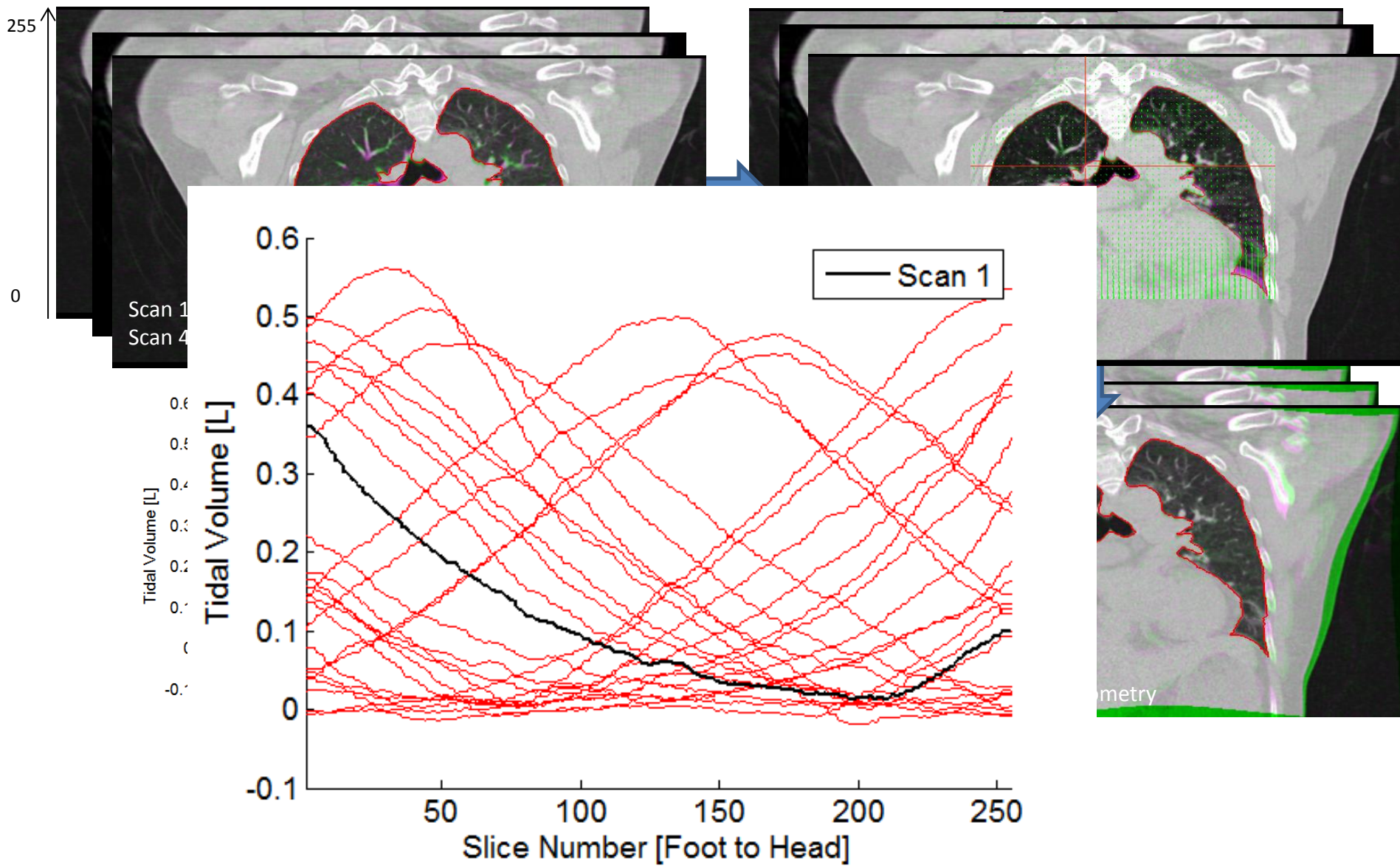
# Image Analysis

- Segment lungs (shear motion)
- Deformable image registration
- Select scan 1 as “reference” scan and measured distortions of other 24 scans relative to it









- 25 Scans registered to Scan 1 geometry
- Average HU values
- Fit HU to bellows signal ( $v$ )



$$+ \quad \bar{X}(v, f) = \bar{X}_0 + \vec{\alpha}(\bar{X}_0)v + \vec{\beta}(\bar{X}_0)f$$

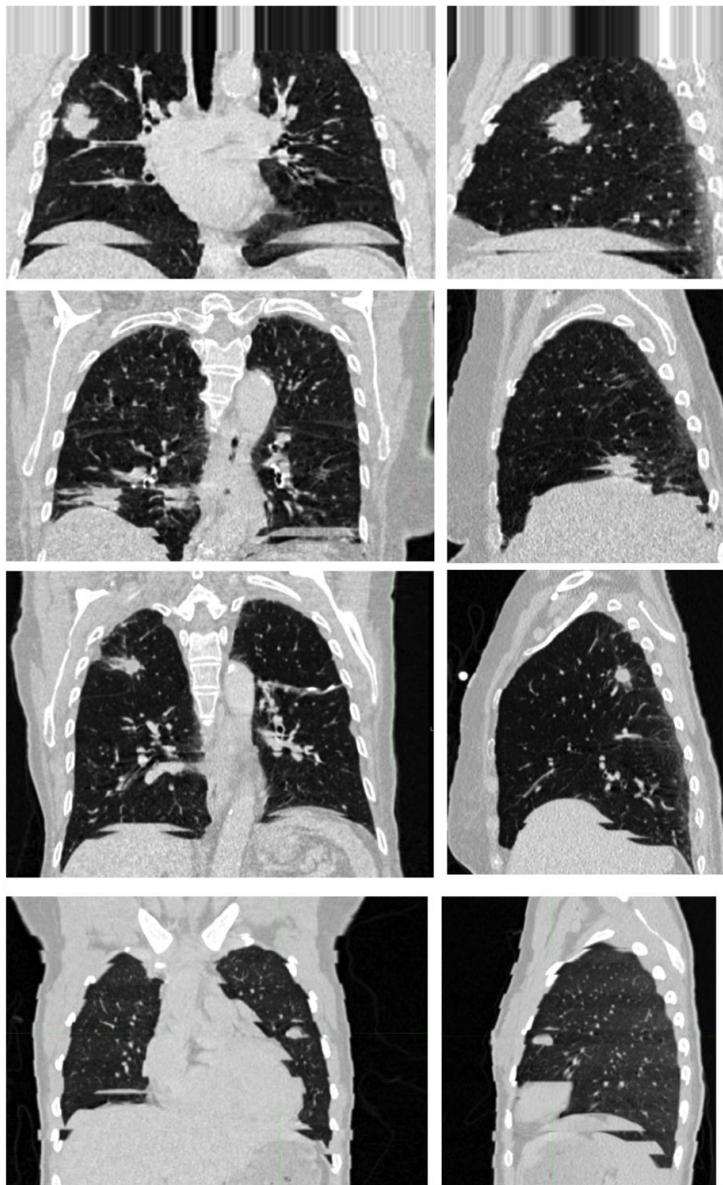
- Deform the low-noise scan from scan 1 geometry to user-selected phase ( $v$  and  $f$ )
- Assign accurate HU values each voxel in the reconstructed images



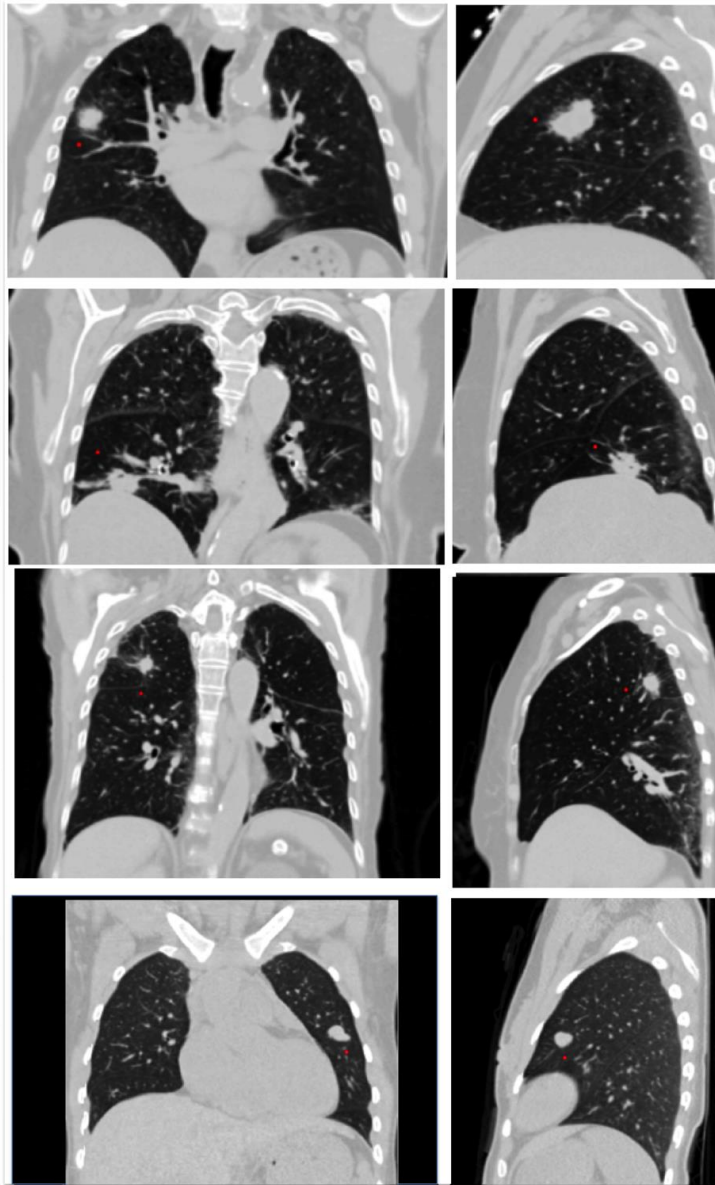
- Psuedo Static Scan 85%ile Inhale



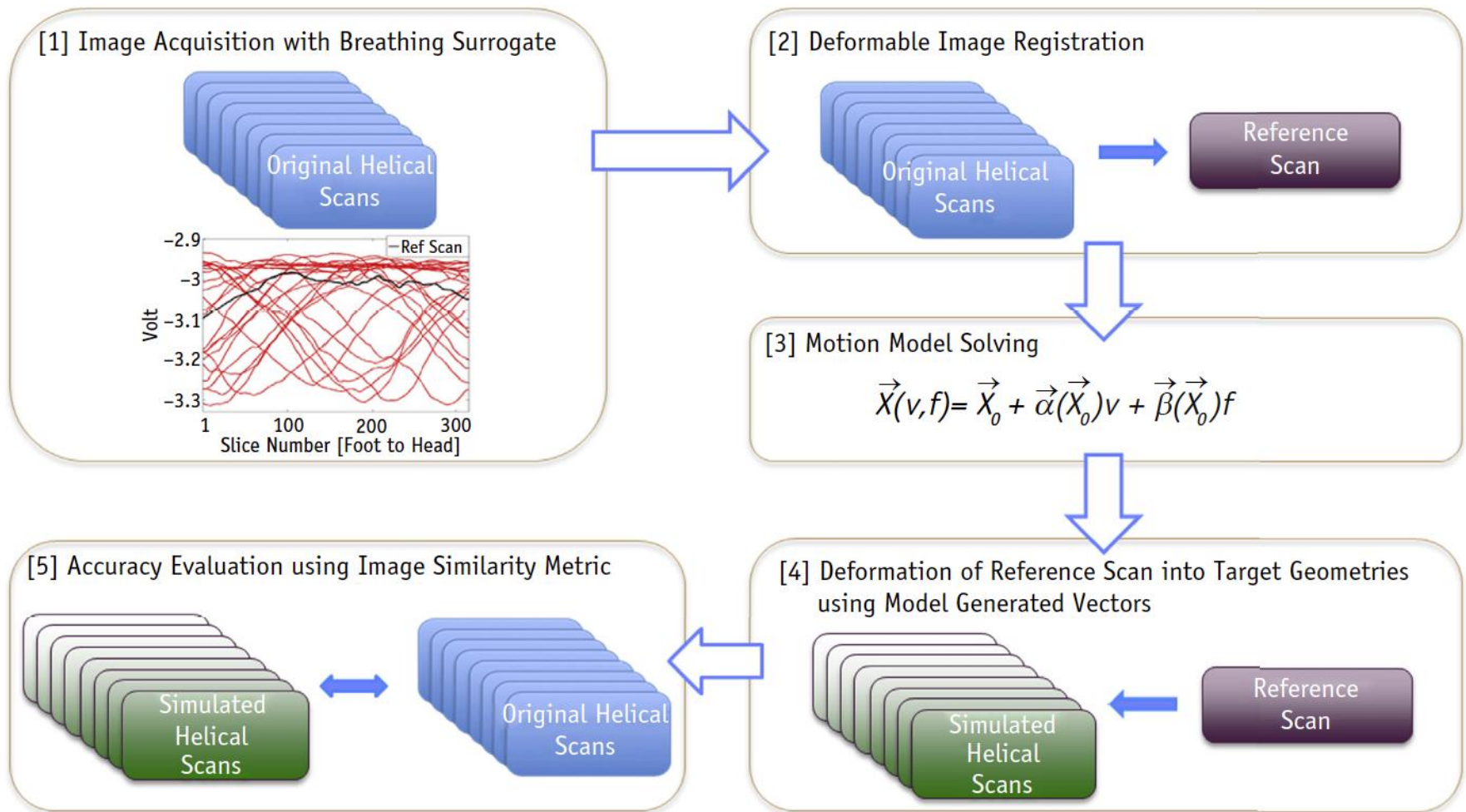
## Clinical Technique



## New Technique

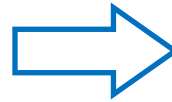
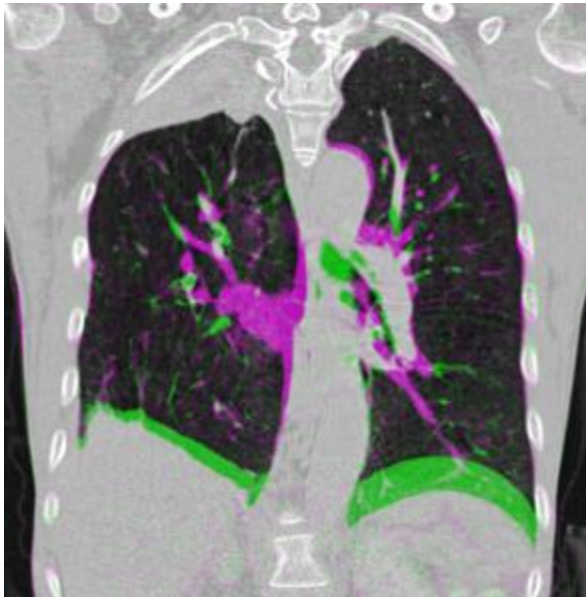


# Pretty, But is it Right?

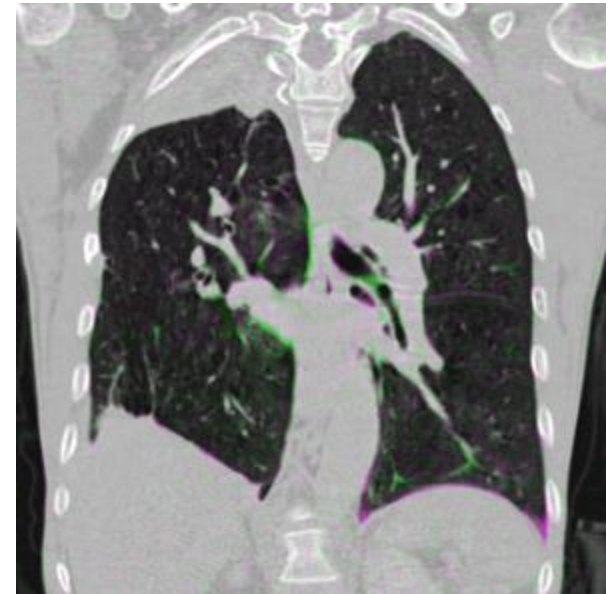


# Overlay – Reconstructed Scan vs. Original Scan

[scan 3] vs. [Reference]

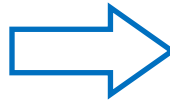
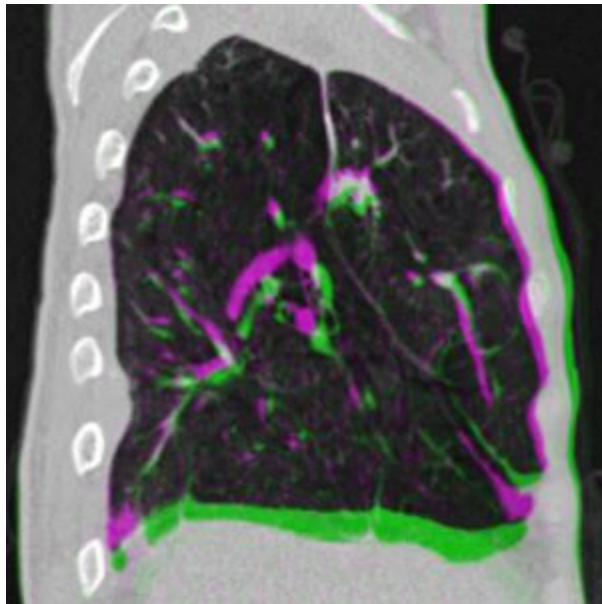


[scan 3] vs. [Reference deformed to scan 3]

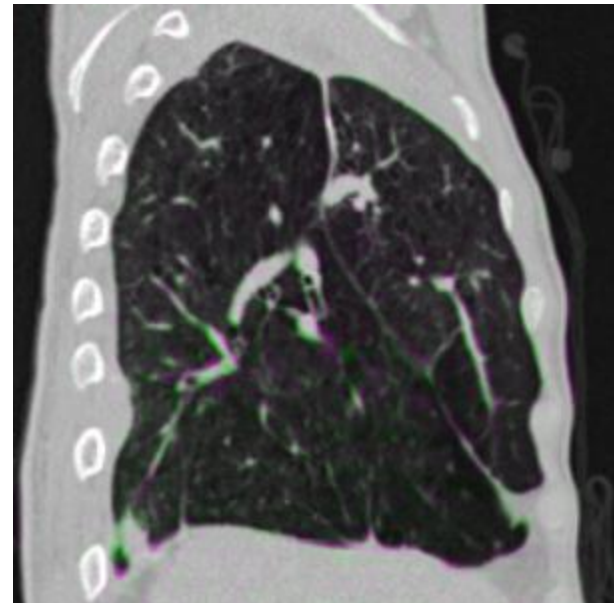


# Overlay – Reconstructed Scan vs. Original Scan

[scan 3] vs. [Reference]



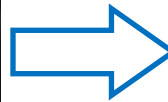
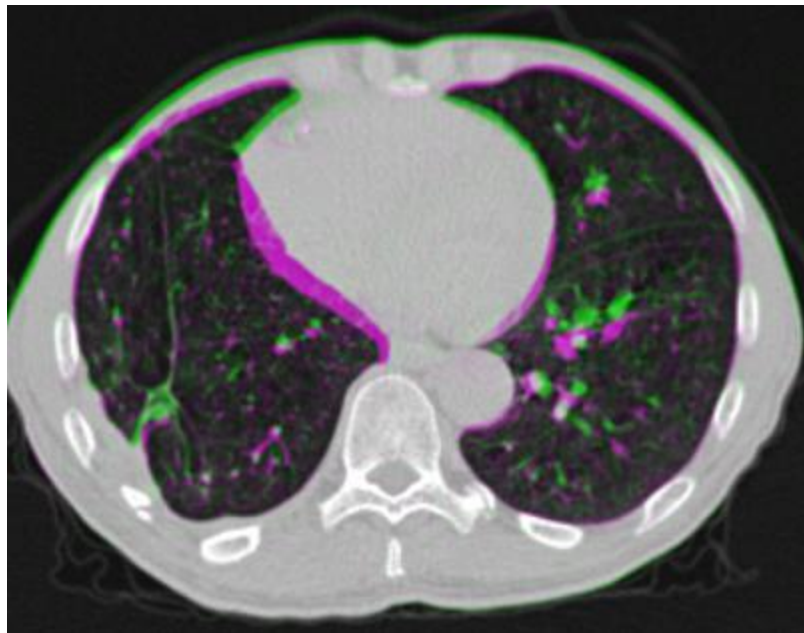
[scan 3] vs. [Reference deformed to scan 3]



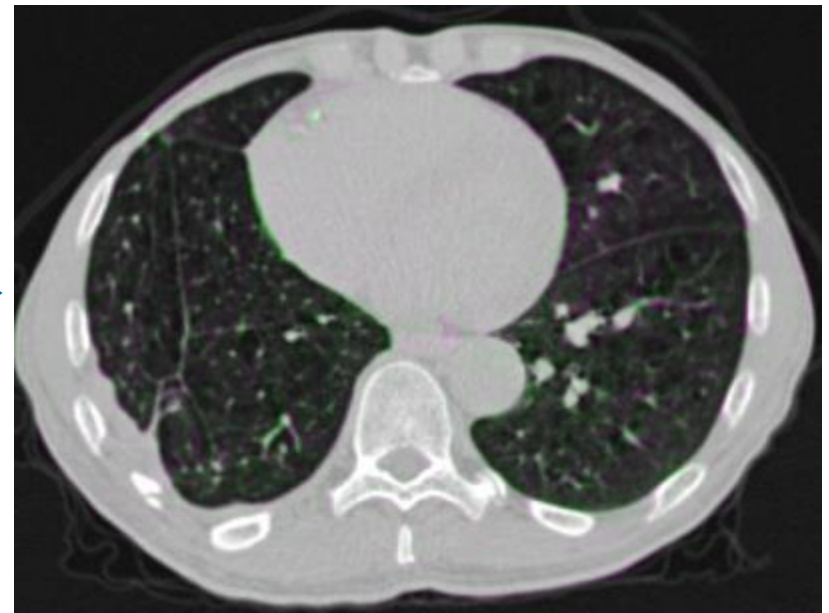


# Overlay – Reconstructed Scan vs. Original Scan

[scan 3] vs. [Reference]

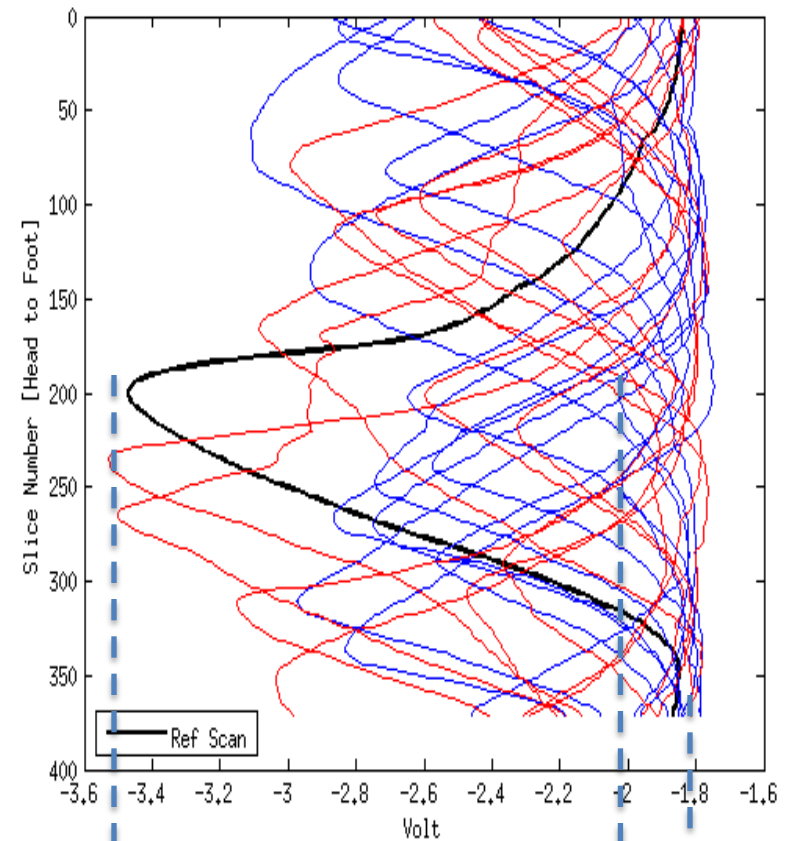
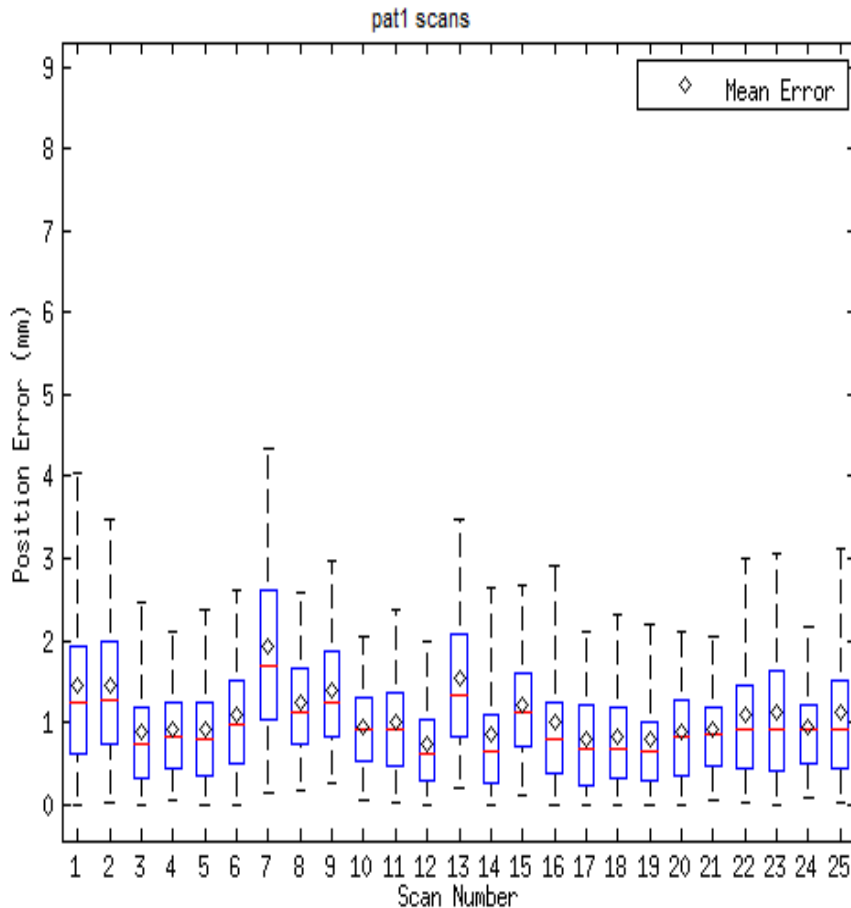


[scan 3] vs. [Reference deformed to scan 3]



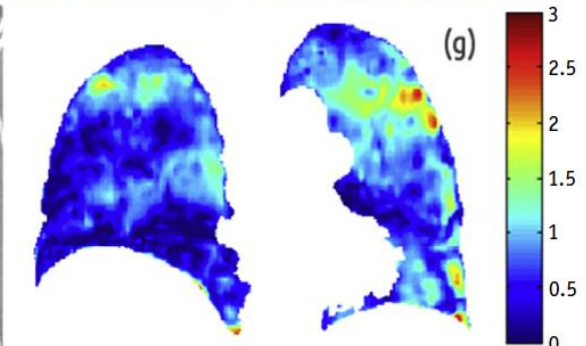
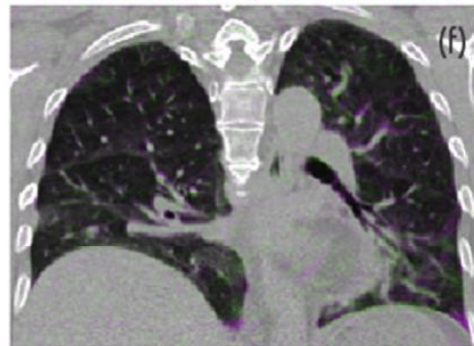
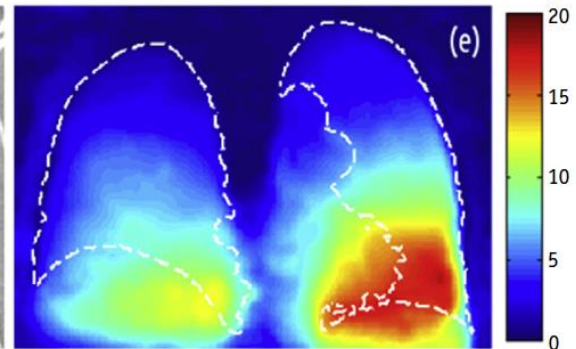
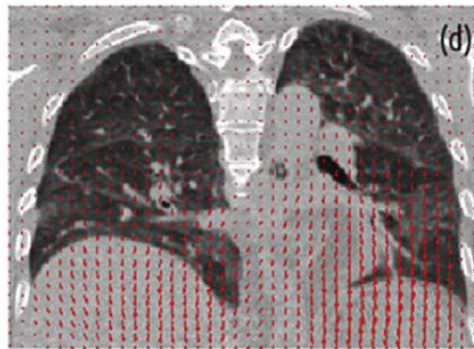
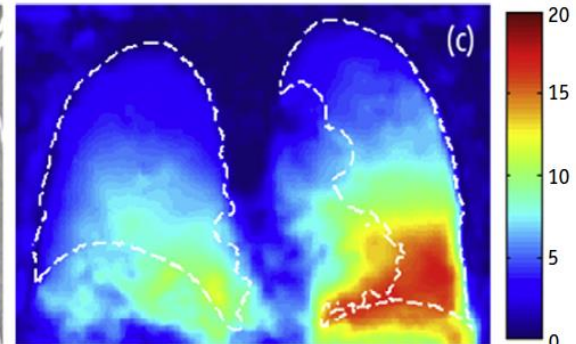
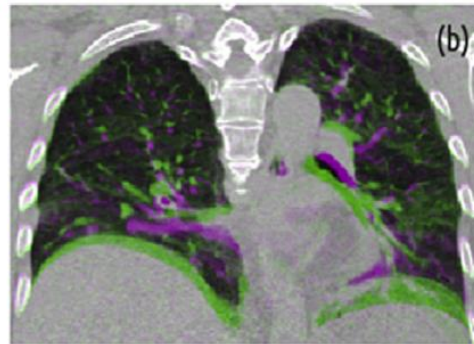
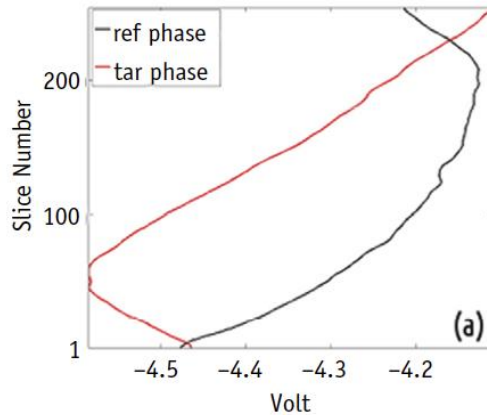


# Error Distribution by the Scans



Factor of 7

# Published Results



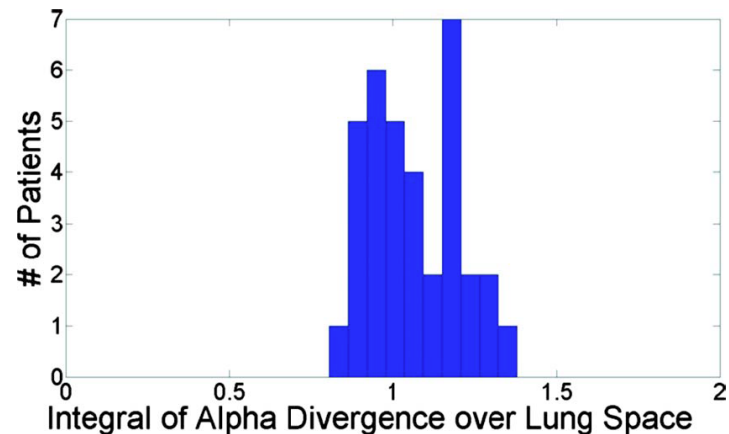
Dou, et al  
Red J 93, 925 (2015)

Mean error  $1.15 \pm 0.37 \text{ mm}$   
95<sup>th</sup> %ile  $2.47 \pm 0.78 \text{ mm}$

# Model Verification

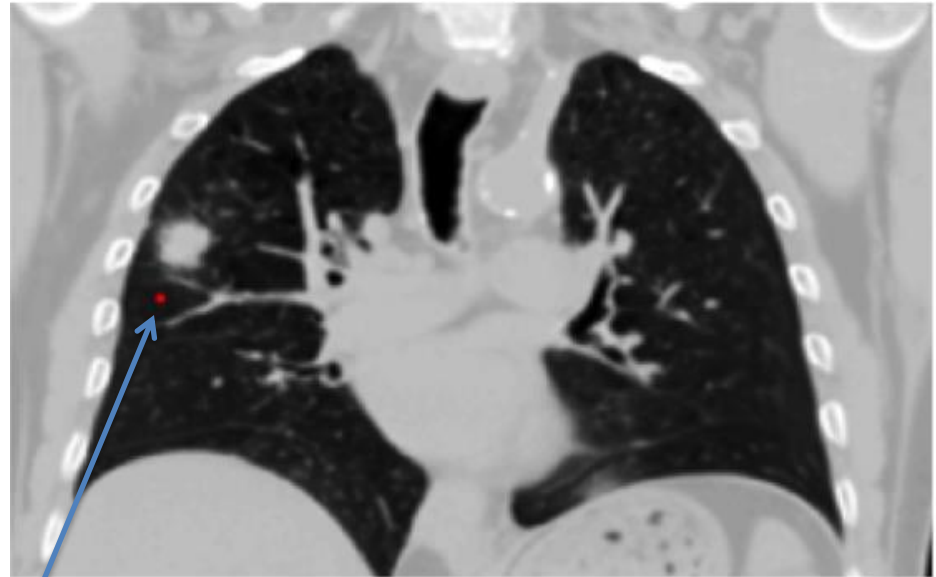
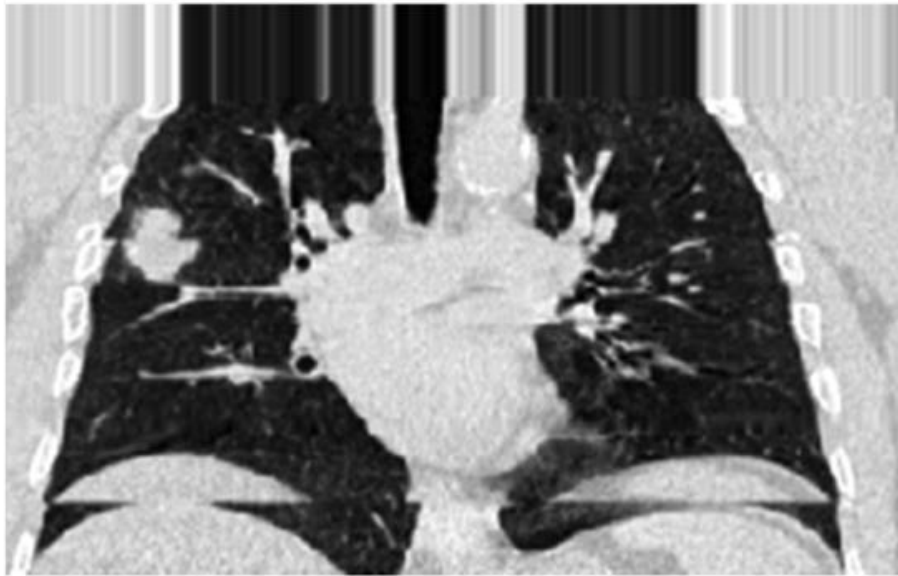
- Model is tied to breathing amplitude
- If amplitude is tidal volume, can use mass conservation to develop quantitation validation

$$\int_V \vec{\nabla} \cdot \vec{\alpha} dV = 1.11.$$



1.06 +/- 0.14

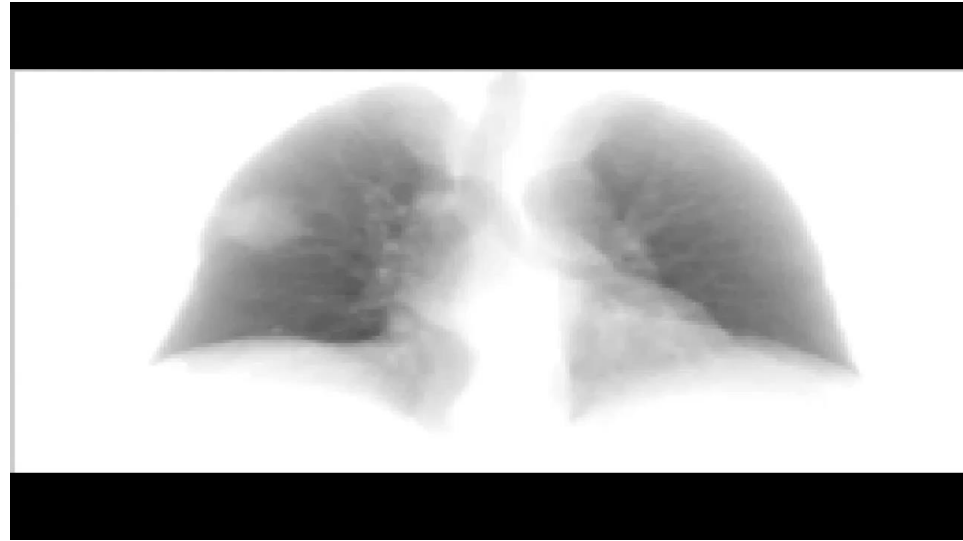
# Results: Interpretation



2mm Diameter Circle

# Benefits of new 4D Approach

- Fast scans, no modification to acquisition
- Average images to allow full use of all irradiated dose
- No sorting artifacts
- User-selected phases (1 image for contouring)
- Deformation maps that can be sent to TPS
- Quantitative
  - Accuracy evaluations
- First Clinical implementation: November 2015!



# Thank You!

- 5D Research Group
  - Daniel A. Low, Ph.D.
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  - Dylan O’Connell
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  - Shyam Jani
  - Xiao Wu
  - Anand Santhanam, Ph.D.
  - Jiulong Liu
  - Lisa Yang
  - Percy Lee, M.D.

